

# Efficient *in vivo* gene expression by *trans*-splicing adeno-associated viral vectors

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Although adeno-associated virus (AAV)-mediated gene therapy has been hindered by the small viral packaging capacity of the vector, *trans*-splicing AAV vectors are able to package twice the size of the vector genome. Unfortunately, the efficiency of current *trans*-splicing vectors is very low. Here we show that rational design of the gene splitting site has a profound influence on *trans*-splicing vector-mediated gene expression. Using mRNA accumulation as a guide, we generated a set of efficient *trans*-splicing vectors and achieved widespread expression of the 6-kb  $\Delta$ H2-R19 mini-dystrophin gene in skeletal muscle of mdx mice, a model for Duchenne muscular dystrophy. The dystrophic phenotype was ameliorated in both adult and aged mice. This demonstrates the use of *trans*-splicing vectors to efficiently express a large therapeutic structural protein. This strategy should be applicable to other large therapeutic genes or large transcription regulatory elements.

AAV is an extremely promising gene therapy vehicle<sup>1–3</sup>. However, being one of the smallest DNA viruses, it cannot carry a large therapeutic expression cassette. A 5-kb genome is considered the upper limit for a single AAV virion<sup>4</sup>. Based on the inherent capacity of AAV genome concatamerization<sup>5–7</sup>, the *trans*-splicing dual vector approach was developed 5 years ago to deliver up to a 10-kb genome<sup>8–11</sup>. Using this approach, a large gene is split into two parts. The 5' gene fragment and a tail-tagged splicing donor sequence are packaged into a donor virus. The 3' gene fragment and a preceding splicing acceptor sequence are packaged into an acceptor virus. Protein expression is achieved through co-infection, viral genome recombination and splicing.

Encouraging preliminary results were achieved for certain secreted proteins such as erythropoietin and Factor VIII<sup>8,12</sup>. Unfortunately, transduction efficiency has been too low to reach the therapeutic level for a structural protein<sup>11</sup>. Moderate improvement was achieved by using novel AAV serotypes or engineering the AAV inverted terminal repeat (ITR) sequence<sup>13,14</sup>. Nonetheless, the challenge remains to translate the exciting potential of *trans*-splicing vectors to a real disease model. Recently, our lab and others have systematically investigated the potential barriers<sup>14,15</sup>. Our results suggest that the

accumulation of mRNA, rather than the simultaneous uptake of both donor and acceptor viruses, is the predominant rate-limiting step<sup>15</sup>.

A unique feature of *trans*-splicing vectors is transcription and splicing across the double-D (dD)-ITR junction in the reconstituted viral genome<sup>6</sup>. We hypothesized that mRNA production in the reconstituted genome is influenced by the DNA sequences flanking the irregular dD-ITR structure. Rational selection of the gene splitting site and optimization of the intron and exon splicing signals may improve overall transduction efficiency of *trans*-splicing vectors. In this study, we tested this hypothesis with the 6-kb  $\Delta$ H2-R19 mini-dystrophin ( $\Delta$ H2) gene.

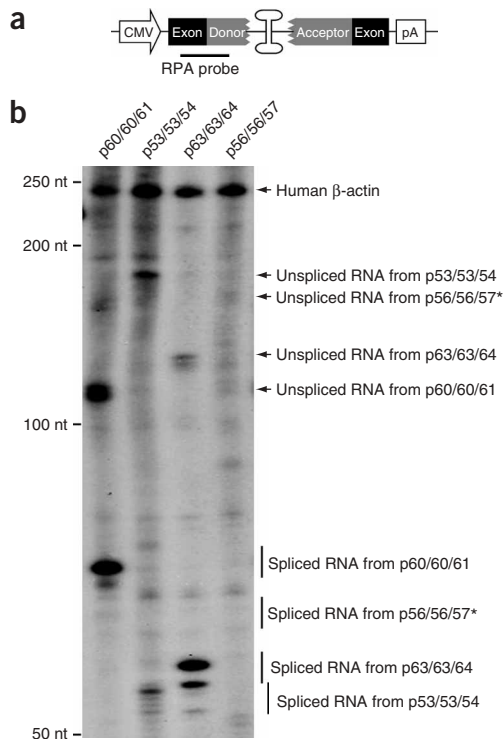
The  $\Delta$ H2 minigene was developed from a truncated, but highly functional, patient-derived gene ( $\Delta$ exon17-48)<sup>16,17</sup>. The patient with the exon 17-48 deletion displayed an extremely mild phenotype and was ambulant beyond age 60 (ref. 16). The  $\Delta$ H2 minigene is nearly identical to the full-length dystrophin cDNA except for a perfectly phased deletion in the rod domain (from hinge 2 to spectrin-like repeat 19). Transgenic expression of the  $\Delta$ H2 minigene completely prevented dystrophy in mdx muscle and resulted in muscle strength indistinguishable from that of the wild-type animal<sup>17</sup>. These studies suggest that the  $\Delta$ H2 minigene may represent a promising alternative to the full-length cDNA, to rescue dystrophic pathology. Because of the large size of the cDNA, the  $\Delta$ H2 minigene represents a great system to explore limitations and improvements in *trans*-splicing AAV vectors.

To determine the optimal gene splitting site, we first screened the splicing signals from a series of endogenous exon/intron/exon junctions in the  $\Delta$ H2 minigene by RNase protection assay (RPA). Considering the size constraint of a single AAV virion, any exon boundary between exons 51 and 65 would be appropriate to divide the  $\Delta$ H2 minigene. We initially selected three sites that have the highest consensus splicing values and the most favorable thermodynamic parameters for U1snRNA binding<sup>18</sup>. These exon/intron/exon junctions are 56/56/57, 60/60/61 and 63/63/64. We also picked the 53/53/54 junction, which has an average U1snRNA binding value of the entire dystrophin gene<sup>18</sup>.

We synthesized a series of mini-cassettes to mold the reconstituted viral genomes. Each cassette contained the flanking exon sequences at the putative splitting site, the endogenous intron splicing signals and

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**Figure 1** Endogenous splicing signal screening. The RPA was used to evaluate splicing and mRNA accumulation of the selected dystrophin exon/intron/exon junctions in the presence of the dD-ITR structure. **(a)** Schematic outline of the constructs used in the RPA (not drawn to scale). The endogenous intron splicing sequences were retrieved from genomic DNA by PCR. The dD-ITR was engineered between the 5' and the 3' splicing signals inside the intron. The location of antisense RPA probes is marked. **(b)** A representative photomicrograph from six independent RPA experiments. The endogenous human  $\beta$ -actin RNA (the control for RPA and loading) was detected by an independent probe added at the same time. \*, the expected location of the RNA transcripts from p56/56/57.

the dD-ITR junction (Fig. 1a). We then examined the splicing profile and mRNA accumulation by RPA (Supplementary Methods online)<sup>15</sup>. The 60/60/61 junction had the best calculated splicing value (Table 1). Interestingly, the 63/63/64 junction, also a well conserved splicing site, showed the highest splicing efficiency in the RPA (Fig. 1b, Table 1). The ratio of spliced to unspliced RNA in p63/63/64 was more than twofold higher than that in p60/60/61. Surprisingly, the 56/56/57 junction was the poorest site. In contrast to the distinctive bands of unspliced and spliced RNA transcripts, our RPA revealed a smear of low molecular weight products from p56/56/57 (Fig. 1b). In addition to quantifying splicing efficiency, we also measured the steady state level of spliced RNA. The 60/60/61 junction yielded the highest level of mRNA, followed by the 63/63/64 junction and the 53/53/54 junction. The 56/56/57 junction produced little detectable spliced transcript (Fig. 1b and Table 1).

The RPA results suggest that the 60/60/61 and the 63/63/64 junctions may represent excellent candidate sites to split the minigene. To test whether the unique sequence organization in these locations

could overcome the mRNA accumulation barrier, we engineered two pairs of *trans*-splicing vectors based on the endogenous splicing signals from introns 60 and 63, respectively (Fig. 2a). The minigene was split precisely between exons 60 and 61, or between exons 63 and 64, as determined by RPA (Fig. 1). Donor and acceptor viruses were packaged in AAV serotype-6 capsid and delivered either individually or together to the tibialis anterior (TA) and the extensor digitorum longus (EDL) muscles of 2-month-old mdx mice (Supplementary Note and Supplementary Fig. 1 online). Mini-dystrophin was not detected in muscles infected with a single vector alone (Figs. 2b and 3b, and Supplementary Fig. 2 online). At 1 month after infection, low levels of the mini-dystrophin protein were found in AV.Donor.63 and AV.Acceptor.63 co-infected muscles (Fig. 2). The 60/60/61 junction yielded the highest level of mRNA in the RPA (Fig. 1). Consistent with this result, *trans*-splicing vectors developed using this junction (AV.Donor.60 and AV.Acceptor.60) yielded significantly higher mini-dystrophin expression (Fig. 2). At 3 months after infection, ~80% (ranging from 46% to 96%) of myofibers were transduced in the injected TA muscles (Fig. 3a, Supplementary Fig. 2 online). Importantly, this high level transduction was observed in the absence of a cellular immune response (Supplementary Fig. 3 online).

To determine the functional competence of mini-dystrophin produced by *trans*-splicing vectors, we first evaluated whether it would assemble the dystrophin-associated glycoprotein complex (DGC). The components in all three DGC subcomplexes (the dystroglycan, the sarcoglycan and the cytoplasmic) were restored to the sarcolemma (Supplementary Fig. 4 online). Consistent with a previous study in the  $\Delta 17$ -48 minigene transgenic mdx mice<sup>19</sup>, neuronal nitric oxide synthase expression was not restored (Supplementary Fig. 4 online).

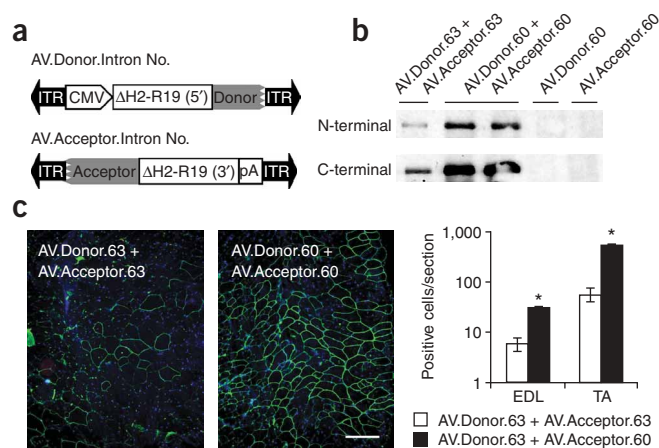
A more stringent test is to determine whether mini-dystrophin produced by *trans*-splicing vectors could ameliorate dystrophic pathology and improve muscle strength. We first examined the therapeutic effect in the EDL muscle of 2-month-old mdx mice. On

**Table 1** The predicted splicing parameters and RPA results

	Exon/intron/exon combination			
	53/53/54	56/56/57	60/60/61	63/63/64
CV <sup>a</sup>	0.90, 0.60	0.84, 0.97	0.94, 0.98	0.95, 0.90
$\Delta DG_{37}^b$	-7.7	-10.4	-11.7	-10.6
Total RNA	68.7 $\pm$ 27.8	2.4 $\pm$ 1.2 <sup>c</sup>	342.2 $\pm$ 24.3 <sup>d</sup>	159.9 $\pm$ 9.4 <sup>c</sup>
Unspliced RNA	20.0 $\pm$ 9.1	1.6 $\pm$ 1.2	87.1 $\pm$ 11.2 <sup>d</sup>	20.4 $\pm$ 9.1
Spliced RNA	48.8 $\pm$ 20.6	0.8 $\pm$ 0.2	255.1 $\pm$ 20.6 <sup>d</sup>	139.5 $\pm$ 6.4 <sup>d</sup>
S/U ratio <sup>e</sup>	2.5 $\pm$ 0.3	1.0 $\pm$ 0.6	3.0 $\pm$ 0.4	7.1 $\pm$ 0.9 <sup>d</sup>
% of splicing	71.1	31.3 <sup>c</sup>	74.5	87.2 <sup>c</sup>

<sup>a</sup>Consensus splicing values (CV) at the 5' and the 3' ends of each indicated intron (from ref. 18). A higher value indicates a better match. <sup>b</sup>Free energy exchange during U1snRNA annealing (Kcal/mole). The more negative the value, the more favorable the annealing. <sup>c</sup>Values are statistically different from each other in the same category ( $P < 0.014$ ). <sup>d</sup>Values are statistically different from other exon/intron/exon combinations in the same category ( $P < 0.016$ ). <sup>e</sup>The ratio of spliced (S) to unspliced (U) RNA transcript.

**Figure 2**  $\Delta$ H2 mini-dystrophin expression from two independent sets of *trans*-splicing AAV vectors. The EDL and the TA muscles of 2-month-old mdx mice were co-infected with  $1 \times 10^{10}$  vector genomes (vg) (for the EDL muscle) and  $2 \times 10^{10}$  vg (for the TA muscle) particles of each pair of *trans*-splicing viruses. Single vector infection (donor or acceptor alone) was also included in the cohort study ( $5 \times 10^9$  vg particles for the EDL muscle and  $1 \times 10^{10}$  vg particles for the TA muscle). Mini-dystrophin expression was evaluated 1 month later. (a) Schematic diagram of  $\Delta$ H2 mini-dystrophin *trans*-splicing vectors (not drawn to scale). The donor virus carries the cytomegalovirus (CMV) promoter, the 5' portion of the  $\Delta$ H2 minigene and the endogenous splicing donor signal (from intron 60 and 63, respectively). The acceptor virus carries the endogenous splicing acceptor signal from the same intron (60 and 63, respectively), the remaining minigene and the polyA sequence. The viruses are accordingly named after the respective intron. (b) Western blot analysis of mini-dystrophin expression in muscle extracts with monoclonal N-terminal (specific for human dystrophin) and C-terminal antibodies, respectively. Each lane is from one infected TA muscle. Different samples were used for the N-terminal and C-terminal immunoblots. (c) Quantification of  $\Delta$ H2 minigene expression by immunofluorescence staining with a human dystrophin-specific antibody. Left panels are the representative photomicrographs from the TA muscles infected with the indicated set of *trans*-splicing vectors. Scale bar, 200  $\mu$ m. Right panel represents mini-dystrophin-positive myofibers per muscle section.  $n = 3-7$  samples for each group. \*, the difference between two sets of *trans*-splicing vectors was statistically significant.



average, co-infection led to mini-dystrophin expression in 49% of myofibers (ranging from 12% to 98%) (Fig. 3b,c). The percentage of centrally nucleated myofibers, a hallmark of muscle degeneration and regeneration, was reduced from 85% in AV.Acceptor.60 infected muscle to 20% in AV.Donor.60 and AV.Acceptor.60 co-infected muscle (Fig. 3c). *Trans*-splicing AAV-treated muscle also showed a trend toward increased sarcolemma integrity and mini-dystrophin-positive fibers were completely protected from membrane damage (Fig. 3b,c). In a physiology assay, we observed a significant improvement in the specific force of *trans*-splicing AAV-treated muscle  $P < 0.018$  (Fig. 3c, Supplementary Note and Supplementary Fig. 1 online). Furthermore, these muscles became more resistant to eccentric contraction-induced injury (Fig. 3c).

Old mdx muscle displays more severe muscle pathology. To further evaluate our *trans*-splicing vectors, we infected the EDL muscles of 1-year-old mdx mice. Surprisingly, efficient transduction was achieved at 6 months after infection (Fig. 3d). On average, the transduction efficiency reached 40% (ranging from 18% to 73%) (Supplementary Fig. 5b online). Despite a quite efficient gene transfer, we only observed moderate improvement in the eccentric contraction assay (Fig. 3d). Other pathology parameters such as central nucleation, fibrosis and macrophage infiltration were not altered (Supplementary Fig. 5 online). This finding suggests that early intervention may be critical for Duchenne muscular dystrophy (DMD) gene therapy. Nevertheless, our results in both adult and aged mdx muscles clearly demonstrated the therapeutic potential of *trans*-splicing AAV vectors for DMD gene therapy.

Until the recent development of dual vector technologies, AAV has been excluded as a candidate vehicle for large therapeutic genes. *Trans*-splicing vectors, though theoretically promising, have so far failed to express a large structure gene at the therapeutic level. We have recently found that the RNA processing represents a crucial barrier to efficient transduction in *trans*-splicing vectors<sup>15</sup>. Boosting the level of accumulated mRNA may represent a promising avenue to improve *trans*-splicing vector-mediated gene expression. To test this hypothesis, we examined splicing efficiency and mRNA production from a series of exon-intron-exon junctions in the 6-kb mini-dystrophin gene. Consistent with the well-documented observation that RNA transcription and splicing are influenced by DNA sequences<sup>20,21</sup>, insertion of the dD-ITR junction to different introns resulted in different effects on

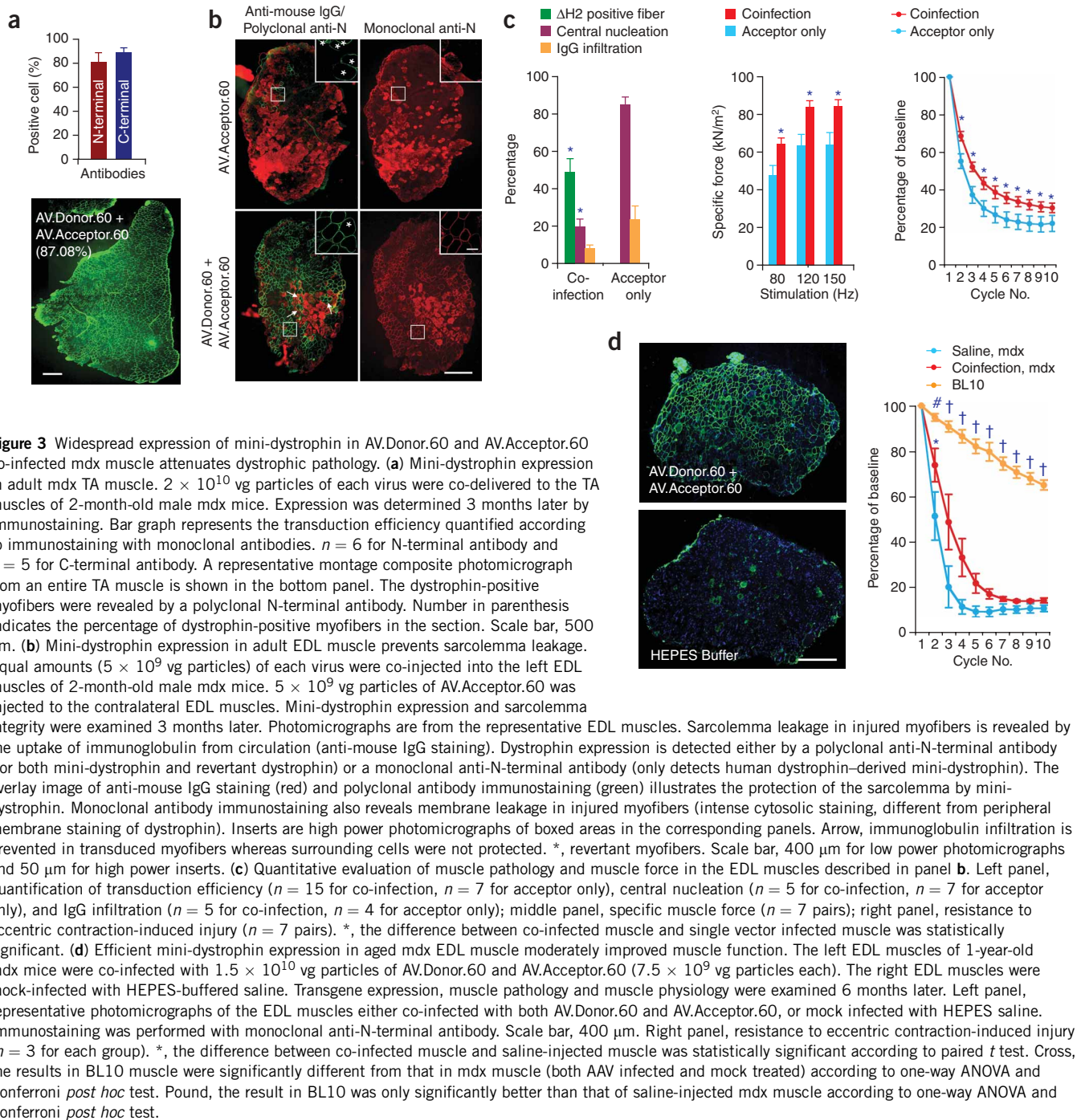
splicing and mRNA accumulation. Intron 63 was the most efficient splicing site whereas intron 60 yielded the highest level of mRNA. The molecular mechanisms underlying this observation remain to be defined, but it may relate to transcription blocking and/or RNA stability<sup>15,22</sup>. We also compared protein production between *trans*-splicing vectors that were split at either intron 60 or intron 63. Both western blot analysis and immunostaining demonstrated a higher expression in the intron 60 splitting vectors. This result strongly suggests that *trans*-splicing vectors should be constructed using the site that yields the highest mRNA.

In summary, we have developed a strategy to rationally design *trans*-splicing AAV vectors. This finding may have a broad impact on developing *trans*-splicing vectors for other large therapeutic genes (such as the cystic fibrosis transmembrane conductance regulator gene and the photoreceptor-specific ATP binding cassette transport gene for the treatment of cystic fibrosis and Stargardt disease, respectively) as well as the use of large complicated transcription regulatory elements in the AAV vector.

## METHODS

**Evaluation of the endogenous splicing signals.** The exon-intron junctions flanking introns 53, 56, 60 and 63 of the human dystrophin gene were amplified by PCR from HEK293 cell genomic DNA (Supplementary Methods online). The double D-ITR junction was derived from a circular AAV genome isolated from infected muscle<sup>15</sup>. The mini-constructs for the RPA were assembled on pcDNA3.1(+) (Invitrogen) (Fig. 1). A total of four plasmids were generated including (in the order of exon/intron/exon) p53/53/54, p56/56/57, p60/60/61 and p63/63/64. The templates for RPA probes were PCR amplified from each respective plasmid and cloned in pGEM3Z (Promega) (Supplementary Methods online). RPA probes (for the dystrophin gene and the endogenous human  $\beta$ -actin gene) were generated by *in vitro* transcription as described before<sup>15</sup>. RPA reaction and RNA signal quantification were carried out according to a published protocol<sup>15</sup>. Constructs generated by PCR amplification were validated by sequencing.

**AAV vector and animal procedure.** Two sets of *trans*-splicing vectors were generated based on the endogenous splicing signals from introns 60 and 63, respectively. Each set included a donor and an acceptor. These vectors were generated by first introducing the corresponding intron splicing sequences in the  $\Delta$ H2 minigene. The intermediate constructs were then inserted into previously described multiple cloning AAV *cis* plasmids (Supplementary Methods online). AAV-6 packaging plasmids (pMTrep2 and pCMVcap6) were



gifts from A. Dusty Miller<sup>23</sup>. Pseudotyped recombinant AAV stocks were generated by quadruple plasmid transfection with the *cis* plasmid, pMTrep2, pCMVcap6 and pHelper (Stratagene) at a ratio of 1:1:3:3 in HEK293 cells. Crude lysate was purified through three rounds of CsCl isopycnic ultracentrifugation and titrated by slot blot as we reported before<sup>24</sup>. All animal experiments were approved by the Animal Care and Use Committee at the University of Missouri and were in accordance with National Institutes of Health guidelines. The mdx mouse strain was originally purchased from the Jackson Laboratory. The experimental mice were obtained from breeding colonies established locally (**Supplementary Note** and **Supplementary Fig. 1** online). Both experimental and breeding mice were housed in a specific-pathogen-free animal facility. AAV was delivered to the EDL and/or

TA muscles of male mdx mice using previously described protocols<sup>24,25</sup>. Both slow- and fast-type myofibers were transduced by AAV-6. However, there seemed to be a trend toward preferential transduction of fast type myofiber (**Supplementary Fig. 6** online).

**Protein expression and morphology.** Mini-dystrophin expression was evaluated by indirect immunofluorescence staining and western blot analysis<sup>26,27</sup>. Antibodies used for these studies include Dys-3 (monoclonal, Novocastra, Newcastle, UK; 1:10 for immunostaining and 1:20 for western blot analysis, specific for human dystrophin N-terminal domain), Dys-2 (monoclonal, Novocastra, 1:30 for immunostaining and 1:100 for western blot analysis, specific for dystrophin C-terminal domain), Mandys 8 (monoclonal, Sigma; 1:100 for immunostaining,

specific for exon 32) and an affinity purified polyclonal anti-dystrophin N-terminal antibody (1:600 for immunostaining only)<sup>17,25</sup>. Muscle microsome preparation was used for western blot analysis. Equal loading was confirmed by Ponceu S staining of the membrane and anti- $\beta$ -catenin immunoblotting of stripped membranes (**Supplementary Methods** online)<sup>28</sup>. The DGC components were evaluated by immunostaining with monoclonal antibodies against  $\beta$ -dystroglycan (Novocastra, 1:50),  $\beta$ -sarcoglycan (Novocastra, 1:50), dystrobrevin (BD Bioscience; 1:200), and syntrophin (Abcam; 1:200). Transduction efficiency was determined by dividing the total number of Dys-3 positive cells (immunostaining) with the total number of myofibers (hematoxylin and eosin (H&E) staining of adjacent section). At least two montage composites of the entire cross sections in the mid-belly were quantified for each muscle sample. The percentage of centrally nucleated myofibers was determined as described before<sup>25</sup>. Standard histochemical procedures were used for HE, Masson trichrome and nonspecific esterase staining.

**Muscle physiology.** The EDL muscle was carefully isolated and mounted on a dual mode servomotor transducer (Aurora Scientific) in Ringer's solution. Muscle stimulation, data acquisition and data analysis were conducted with DMC/DMA software (Aurora) (**Supplementary Methods** online). The absolute muscle force was measured at 80, 120 and 150 Hz. The specific force was calculated by dividing the value of absolute force with muscle cross-sectional area (**Supplementary Methods** online)<sup>25</sup>. The eccentric contraction assay was performed according to a published protocol<sup>25</sup>.

**Statistical analysis.** Data are presented as the mean  $\pm$  s.e.m. and analyzed with SPSS software. In studies involving two groups, comparisons were made using two-tailed *t*-tests (paired or unpaired depending on the situation). In studies involving multiple groups, comparisons were made using one-way ANOVA followed by Bonferroni *post hoc* test. Differences were considered significant when  $P < 0.05$ .

Note: Supplementary information is available on the Nature Biotechnology website.

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#### COMPETING INTERESTS STATEMENT

The authors declare that they have no competing financial interests.

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